

Background

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Conducting airways <2mm in diameter account for only about 20% of total air flow resistance in the normal lung, however these same airways become the major site of obstruction in COPD⁽¹⁾. Furthermore, using a combination of clinical multi-detector computed tomography (MDCT) and micro-CT it has been shown that narrowing and loss of terminal bronchioles contributes to peripheral resistance in COPD⁽²⁾. Due to the age-related prevalence of COPD, here we use a structure-based mathematical model to study how FEV, changes in response to loss of terminal bronchioles in combination with age-related decline in lung tissue elastic recoil.

Methods

- 6 normal healthy subjects (3 M, 3 F). Table 1 shows a subject summary.
- Structure-based lung and airway models from MDCT⁽³⁾ (See Figure 1). Finite deformation elasticity for tissue displacement and elastic recoil⁽⁴⁾.
- Airway tree embedded in model lung tissue.
- Wave-speed model⁽⁵⁾ to predict maximum flow at all lung volumes. Viscous pressure drop using relationship developed by Collins et al.⁽⁶⁾.
- Airway compliance determined using Lambert's model⁽⁵⁾.
- Model initiated at total lung capacity (TLC) from which a forced expiration for 1 second (FEV₁) was simulated (time interval 0.05s). 'Ageing' of lung simulated by: 1. decreasing lung tissue elastic recoil,
- and 2. removing terminal bronchioles. Baseline model generated for one healthy 63 year old male. Subject
- extrapolated to other ages that were studied here.



Forced expiration in the baseline model

Figure 2 shows baseline model results for subject M1 along with measurements from pulmonary function tests. Parameterisation of the baseline model by fitting peak muscle (driving)

pressure and rate of decrease of airway diameter with decreasing order. Variation between measurements and computational results for all six subjects are: FEV₁ 2.4 ± 1.2 % ,FEF₂₅₋₇₅ 4.3 ± 1.8%, P_{ef} 0.3 ± 0.3%



Figure 2: Description index results insidated in solution (Pi_1: (9), initiated insidiate expiratory flow volume curve (blue), and measured peak expiratory flow (Pe₀, red) and forced vital capacity (FVC, green). (b) Expired volume against time, to illustrate measured FEF_{25/75} (purple) and FEV₁ (red), and location of <u>model data points</u> for FEF_{25/75} calculation.

Loss of tissue elastic recoil

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Figure 3 shows model prediction of decrease in FEV, with 'age' as a % of FEV₁ calculated at 25 years for each subject (males green, females blue). Lung tissue compliance by decade identical for all subjects. Muscle pressure and airway dimensions parameterised to baseline young data. Loss of tissue elastic recoil in the model results in decreased FEV₁ and increased inter-subject variability.

The models are in concordance with the literature, including an – on average – more rapid decline in FEV_1 with age in females.



Removing terminal bronchioles

- Figure 4 shows the effect on predicted FEV_1 of removing terminal bronchioles in two subjects. Airways removed 20% at a time, by removing every nth airway from the model. i.e. approximately homogeneously.

 Also shown (horizontal lines) are measured FEV₁, FEV₁ predicted from reference equations, and 80% predicted at 25 years of age.

 Note that in F1 the measured FEV₁ was < predicted; removal of only 20% terminal bronchioles was sufficient to decrease FEV₁ below 80% predicted.

In M2 a loss of 80% of the terminal bronchioles was required in order to reach the 80% predicted FEV_1 threshold.



Figure 4. Decide in model simulated FEV, with removal of terminal boarchieles in (a) subject M2. The key lists the proportion of terminal branchieles remaining in the model, thorizontal lines are shown for measured FEV, $(---)^{-1}$, FEV, predicted from reference equations (.........) and 80% of predicted FEV; $(---)^{-1}$,

Loss of elastic recoil & terminal bronchioles

Figure 5 compares two causes of FEV, decline.

Removing 50% of the terminal airways without a change in elastic recoil from the 25 years value (green) decreases FEV₁ by < 20%.

Decreasing elastic recoil to the 75 years value without removing terminal airways decreases the FEV1 more in females than males (blue). Results show more subject variability.

 Removing 50% of terminal airways from the model with 75 years elastic recoil decreased FEV, by 10-20%, with largest decrease in males.



Figure 5. Comparison of: change in FEV, (with respect to its value at age 25 years) due to loss of elastic recoil to the 75 years level (blue), loss of terminal bronchioles from the 25 years lung (green), loss of terminal bronchioles from the 75 years lung (purple). 80% FEV, predicted at 75 years is shown for comparison (orange).

Modelling Older Subjects

- Figure 6 shows baseline results for a 63 year old healthy, male subject.
 Parameterisation of baseline model using peak muscle driving pressure, rate of decrease of airway diameter, maximum expiratory pressure (from PETs) to measured values at ane 63.
- Change in lung tissue compliance specified to be the same as that defined earlier at age 65 for younger subjects.
- % decrease in muscle pressure equivalent to that from previous study.
 No removal of terminal airways.
- No removal of terminal allways.
- + Model prediction error results: ${\rm FEV}_1$ 12.5%, ${\rm FEF}_{\rm 25-75}$ 56.6%.
- Large discrepancy between calculated and actual PFTs. Airway closure not incorporated into model, model therefore over-predicting results.



Figure 6. Benchmark plots for healthy 63 year old. (a) shows volume flow plot for calculated solution (green) and PFT results (blue) for subject. (b) shows time volume plot from model (blue), calculated FEF₃₋₃₂ (red) and actual FEF₃₋₃₂ value from PFTs (green).

Figure 7 shows the extrapolated results for older subject at other decades.

Results for changes in elastic recoil and muscle pressure only.

Extrapolated FEV, at 25 years of age is 104% predicted for subject based on subject's height and age. (Subject's FEV₁ is 105% predicted at age 63) Figure 8 shows proportions of driving pressure for baseline solution indicating that the most sensitive subjects have smaller proportion of driving pressure contributed from muscle.



Figure 7. Extrapolated results for older subject at decade intervals. Results overlaid on previous results for healthy young subjects (dashed lines). Figure 8. Relative proportions of recoil and muscle pressure combining to generate required driving pressure for P_{ef} solution.

Summary & Conclusions

The model suggests that significant variation in decline of FEV₁ across subjects with age can be attributed to loss of elastic recoil interacting with the subject's specific airway geometry.

Removing terminal bronchioles caused decline of FEV, and increased the age-dependent inter-subject variability, however without an accompanying decline in elastic recoil, very large numbers of terminal airways must be lost before FEV₁ decreases below the threshold of 80% predicted.

Removal of terminal bronchioles had a more consistent effect across subjects (Figure 5) compared with loss of elastic recoil. Women were – on average – more sensitive to loss of recoil than men.

Large decreases in tissue elasticity and numbers of terminal airways are possible before threshold for disease is reached (FEV₁ < 80% predicted).

 The results support the hypothesis that large numbers of terminal airways can be lost with age, without detection on forced spirometry.

Acknowledgements

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